

Single-voxel direct Fourier reconstruction of spiral Fourier velocity encoding data on GPGPUs

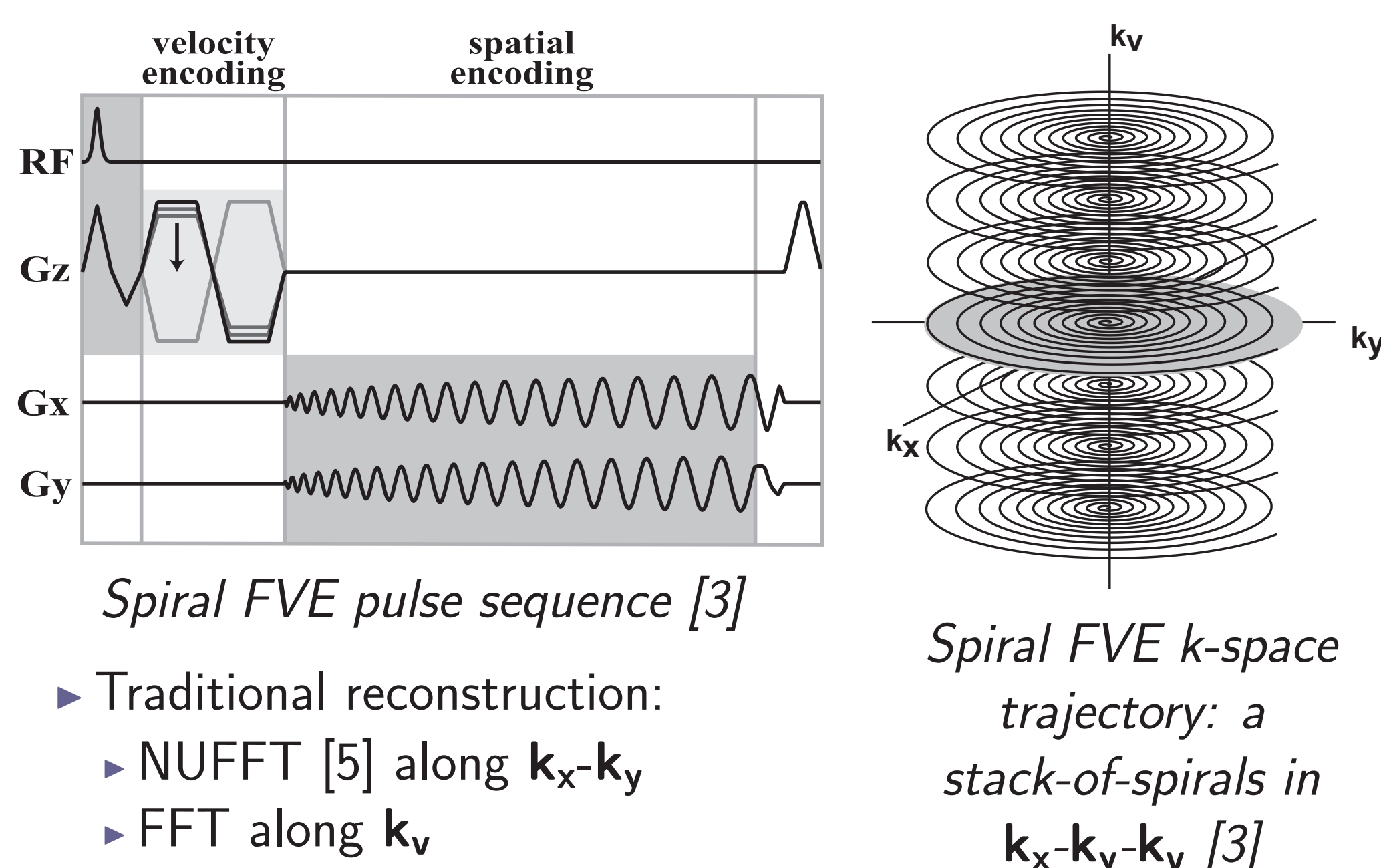
Thales Henrique Dantas (thaleshd@gmail.com)
João Luiz Azevedo de Carvalho (joaoluiz@pgea.unb.br)

Medical Imaging and Signal Processing Group
Department of Electrical Engineering
University of Brasília, Brasília-DF, Brazil

Introduction

- ▶ Phase contrast: fast, but has issues with partial voluming [1]
- ▶ Fourier velocity encoding [2]: robust to partial voluming, but slow
- ▶ Spiral FVE [3]: fast acquisition, but long reconstruction time
 - ▶ High dimensionality + non-Cartesian sampling = SLOW!
- ▶ We are interested in $\mathbf{m}(\mathbf{v}, \mathbf{t})$ for small ROIs, but the entire $\mathbf{m}(\mathbf{x}, \mathbf{y}, \mathbf{v}, \mathbf{t})$ matrix is calculated
- ▶ We propose single-voxel direct Fourier transform (DrFT) [4] for reconstruction of spiral FVE data
 - ▶ DrFT allows reconstruction of individual voxels
 - ▶ GPGPU implementation further accelerates computation
 - ▶ Seemingly instantaneous spiral FVE reconstruction!

Spiral FVE



- ▶ Traditional reconstruction:
 - ▶ NUFFT [5] along \mathbf{k}_x - \mathbf{k}_y
 - ▶ FFT along \mathbf{k}_v

Proposed Reconstruction

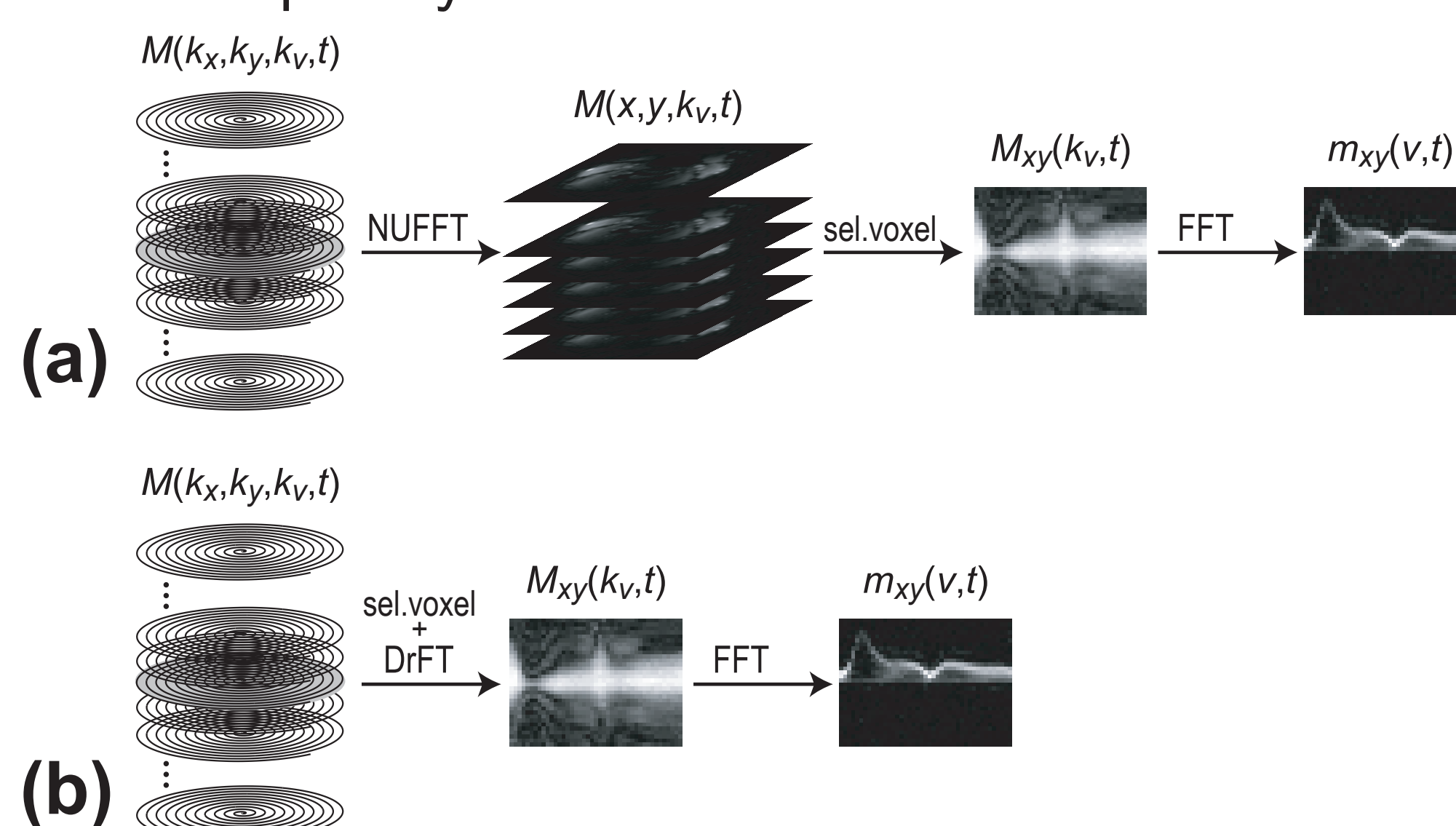
- ▶ K-space dimensionality is reduced by calculating $\mathbf{M}(\mathbf{k}_v, \mathbf{t})$ for a select voxel at position (\mathbf{x}, \mathbf{y}) using the DrFT [4]:

$$\mathbf{m}_{xy} = \sum_{n=0}^{N-1} \mathbf{W}_n \mathbf{M}_n e^{j2\pi(\mathbf{x}u_n + \mathbf{y}v_n)}$$

- ▶ \mathbf{N} is the total number of k-space samples
- ▶ \mathbf{M}_n is the data acquired at k-space position $(\mathbf{u}_n, \mathbf{v}_n)$
- ▶ \mathbf{W}_n is the weight attributed to that k-space position
- ▶ Single-voxel computation reduces DrFT's complexity by 99.99%!
 - ▶ Single-voxel FFT would still require gridding of the entire k-space
 - ▶ Single-voxel NUFFT is not practical, because NUFFT is an iterative algorithm
- ▶ $\mathbf{M}_{xy}(\mathbf{k}_v, \mathbf{t})$ matrices from each coil element are combined using sum-of-squares
- ▶ $\mathbf{m}_{xy}(\mathbf{v}, \mathbf{t})$ is obtained by 1D-FFT along \mathbf{k}_v

Experimental Methods

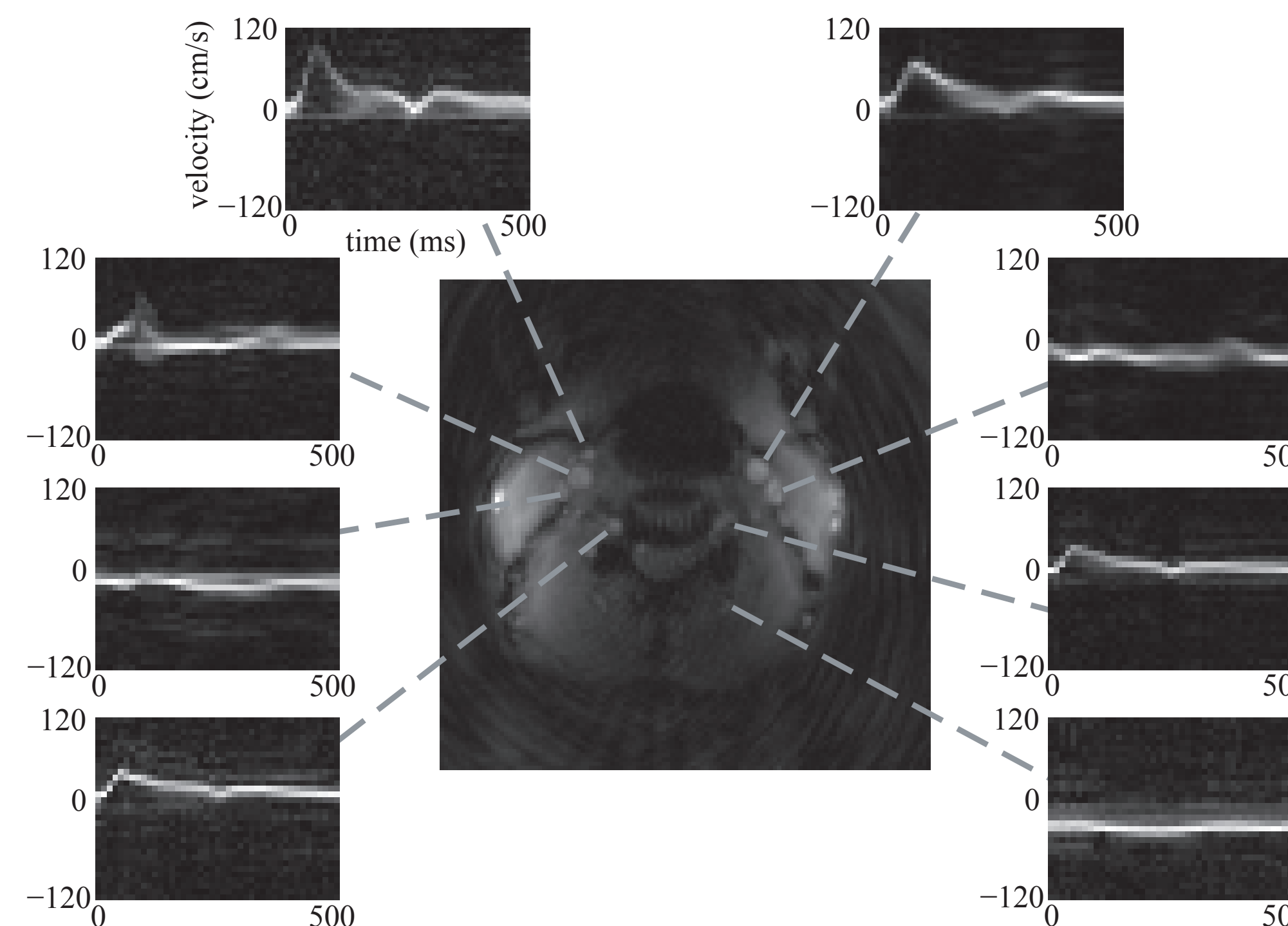
- ▶ Data were reconstructed on an Intel 2.9 GHz Core i7 CPU with an Nvidia GTX570 graphics card, running MATLAB on Linux
- ▶ Single-voxel DrFT was implemented in MATLAB, using segments of code written in CUDA, the parallel computing architecture developed by Nvidia for its GPUs



Reconstruction of spiral FVE data using:
(a) NUFFT; (b) single-voxel DrFT

Reconstructed Data

- ▶ Multi-slice CINE spiral FVE scans
- ▶ Spatial resolution: $1.4 \times 1.4 \times 5 \text{ mm}^3$
- ▶ 8 variable-density spiral readouts (4 ms each)
- ▶ Velocity resolution: 5 cm/s (32 velocity encodes)
- ▶ Temporal resolution: 12 ms (43 cardiac phases)
- ▶ 5 axial slices
- ▶ Scan time: 2.4 min/slice (256 hbs @ 105 bpm)



Time-velocity distributions for select voxels of interest from an axial slice prescribed at the neck of a healthy volunteer

Results and Discussion

- ▶ Reconstruction using NUFFT required 1 minute per slice (5 minutes total)
 - ▶ Only a tiny fraction of the voxels contains flows of interest, but distributions are calculated even for voxels containing no signal or only static material
 - ▶ Requires considerable amount of RAM memory: 1.4 GB for a $115 \times 115 \times 5 \times 32 \times 43$ $\mathbf{m}(\mathbf{x}, \mathbf{y}, \mathbf{z}, \mathbf{v}, \mathbf{t})$ matrix
- ▶ Single-voxel DrFT was able to reconstruct the spiral FVE data in only 5 seconds (per voxel)
- ▶ The CUDA implementation of single-voxel DrFT was able to reconstruct the data in only 135 ms! (per voxel)

Conclusion

- ▶ Single-voxel DrFT allows seemingly instantaneous reconstruction of spiral FVE data
- ▶ The use of GPGPUs for DrFT computation provided a 37-fold reduction in reconstruction time, compared with the CPU implementation of the same reconstruction algorithm
- ▶ Single-voxel DrFT can be used for any non-Cartesian FVE method

References

- [1] Tang C et al. JMRI 3:377, 1993
- [2] Moran PR. MRI 1:197, 1982
- [3] Carvalho JLA, Nayak KS. MRM 57:639, 2007
- [4] Maeda A et al. IEEE TMI 7:26, 1988
- [5] Fessler JA, Sutton BP. IEEE TSP 51:560, 2003

Financial Support

- ▶ PAEX/CAPES
- ▶ PIBIC/UnB/CNPq
- ▶ DEG/UnB
- ▶ PGEA/ENE/FT/UnB
- ▶ Edital MCT/CNPq 014/2010 – Universal